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- Image noise
- 2D FIR filters
- Moving average filters
- Spatial filters
- Median filters
- Digital filters based on order statistics
- Adaptive order statistic filters
- Anisotropic Diffusion
- Image interpolation
- Neural image filtering





Image noise

White additive noise:

x(i,j) = s(i,j) + n(i,j),

White multiplicative noise:

x(i,j) = s(i,j)n(i,j),

White signal-dependent noise:

 $x(i,j) = s^{\gamma}(i,j)n(i,j),$

 Noise can have various distributions: Gaussian, uniform, Laplacian.

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Image noise



Salt-pepper noise consists of black and/or white image impulses:

 $g(i,j) = \begin{cases} z(i,j), & \text{with probability} & p. \\ f(i,j), & \text{with probability} & 1-p. \end{cases}$



Image noise

- Uniform noise has a *shorttailed* probability distribution.
- Laplacian noise has a *longtailed* probability distribution.
- Gaussian noise is at the borderline between long- and short tailed probability distributions.





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2D FIR Digital Filters



The output of a 2D FIR filter is given by a *linear convolution*:

$$y(n_1, n_2) = \sum_{k_1=0}^{M_1-1} \sum_{k_2=0}^{M_2-1} h(k_1, k_2) x(n_1 - k_1, n_2 - k_2).$$

for a *filter window* (region of support) $[0, M_1 - 1] \times [0, M_2 - 1]$.

For centered filter window $[-v_{1, v_1}] \times [-v_{2, v_2}], M_i = 2v_i + 1, i = 1, 2$:

$$y(n_1, n_2) = \sum_{k_1 = -\nu_1}^{\nu_1} \sum_{k_2 = -\nu_2}^{\nu_2} h(k_1, k_2) x(n_1 - k_1, n_2 - k_2).$$



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2D FIR Digital Filters

Moving Average filter:



$$y(n_1, n_2) = \left(\frac{1}{M_1 M_2}\right) \sum_{k_1 = -\nu_1}^{\nu_1} \sum_{k_2 = -\nu_2}^{\nu_2} x(n_1 - k_1, n_2 - k_2),$$

where
$$M_i = 2v_i + 1$$
, $i = 1, 2$.

Properties:

- It is a linear FIR *low-pass filter*.
- It tends to blur edges and image details (e.g., lines, fine texture).
- It degrades image quality, particularly for large filter windows.

Moving Average Filter





 3×3 arithmetic moving average filter structure.



Moving Average Filter





 5×5 moving average image filtering [PIT2000].



2D FIR Digital Filters

Moving average filter properties:

• It is optimal in removing additive white Gaussian noise:

$$f_X(x) = \frac{1}{\sqrt{2\pi\sigma}} \exp\{-\frac{(x-\mu)^2}{2\sigma^2}\}.$$

• Arithmetic mean \bar{x} is the optimal estimator of location μ , as it minimizes the L_2 norm:

$$\sum_{i=1}^n (x_i - \bar{x})^2 \to \min.$$



L_p Mean Filter L_p mean filter:



$$y(n_{1}, n_{2}) = \frac{1}{M_{1}M_{2}} \left(\sum_{k_{1}=-\nu_{1}}^{\nu_{1}} \sum_{k_{2}=-\nu_{2}}^{\nu_{2}} x^{p}(n_{1}-k_{1}, n_{2}-k_{2})\right)^{1/p}$$

where
$$M_i = 2v_i + 1$$
, $i = 1, 2$.

Properties:

- For large values, it tends to the maximum filter.
- L₂ mean filter is optimal in removing Rayleigh noise (e.g., for ultrasound images).



L_p Mean Filter



a) Ultrasound image; b) Output of an L_2 filter [PIT2000].



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Gaussian smoothing is performed by the 2D filter kernel:

$$g(x,y) = \frac{1}{2\pi\sigma^2} e^{-\frac{x^2 + y^2}{2\sigma^2}}.$$

- This kernel has zero mean.
- σ : standard deviation of the Gaussian kernel.
- The Gaussian kernel has low-pass frequency characterics: $G(\omega_x, \omega_y) = e^{-2\pi^2(\omega_x^2 + \omega_y^2)\sigma^2}.$
- It can be used to blur images and remove detail and noise.
- The degree of smoothing is determined by σ .





 5×5 discrete approximation of a Gaussian kernel for $\sigma = 1$.





Unsharp Filter enhances image edges and other high frequency image features, by:

- subtracting a smoothed version of the image from the original to create an edge image.
- Adding the amplified edge image on the original image.

$$f_u(n_{1,n_2}) = f(n_{1,n_2}) + kg(n_{1,n_2}).$$

$$g(n_{1,n_2}) = f(n_{1,n_2}) - f_s(n_{1,n_2}),$$

- $f(n_1, n_2)$: original image.
- $f_s(n_1, n_2)$: smoothed version of $f(n_1, n_2)$.
- $g(n_1, n_2)$: edge image.
- $f_u(n_1, n_2)$: output image.

• k: scaling constant between 0.2 and 0.7.



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Unsharp Filter



Block diagram of the unsharp filter.





Conservative smoothing assumes that noise has a high spatial frequency.

- It can be attenuated by a local operation which ensures pixel intensity consistency in local image neighborhoods.
- It ensures that pixel intensities are bounded within the intensity *range* of its neighbors, defined by their *minimum* and *maximum* intensity values.
- If the central pixel intensity lies within the intensity range of its neighbors, it remains unchanged.
- If it is greater/smaller than the maximum/minmum value, it is set equal to the maximum/minimum value, respectively.

Conservative smoothing



• The central pixel intensity is 150, so it will be replaced with the maximum intensity value (127) of its 8 nearest neighbors.

123	125	126	130	140
122	124	126	127	135
118	120	150	125	134
119	115	119	123	133
111	116	110	120	130

Conservative smoothing in a local pixel neighborhood.



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 $x_i, i = 1, ..., n, n = 2\nu + 1$:



$$x_{(1)} < x_{(2)} < \dots < x_{(n)}$$

 $\sum |x_i - \text{med}| \to \text{min.}$

- $x_{(1)}$: *minimum*, $x_{(n)}$ *maximum* data samples.
- Median is a special type of order statistics.
- It minimizes the L_1 norm:



2D median filter:



 $y(i, j) = med\{x(i + r, j + s), (r, s) \in A, (i, j) \in \mathbb{Z}^2\}.$

Median filter properties:

- They have low-pass characteristics and remove additive white noise.
- They are very efficient in the removal of:
 impulsive noise,
 noise with long-tailed distribution (e.g., having Laplacian distribution).



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Median filter properties:

- Median becomes corrupted, if more than 50% of the data samples are outliers.
- Median *robustness* renders it very suitable for impulse noise filtering.
- Median filtering preserves and, possibly, enhances image edge sharpness.
- Median filter smooths noise in homogeneous image regions but tends to produce regions of constant or nearly constant intensity (blobs).













a) Baboon image corrupted by mixed impulsive noise; b) 7×7 median filter output; c) 7×7 moving average filter output [PIT2000].



Separable 2D median filter:



1D median filtering of length n=2v+1 along image rows and columns:

$$y_{i,j} = med(z_{i,j-v}, ..., z_{i,j}, ..., z_{i,j+v}),$$

$$z_{i,j} = med(x_{i-v,j}, \dots, x_{i,j}, \dots, x_{i+v,j}),$$

- Low computational complexity, compared to non-separable median filter:
 - It sorts *n* numbers two times, instead of ordering n^2 numbers.



Recursive median filter:



 $y_{i,i} = med(y_{i-\nu}, \dots, y_{i-1}, x_i, \dots, x_{1+\nu}).$

- Its output tends to be much more correlated, than that of the standard median filter.
- Recursive median filters have higher immunity to impulsive noise than the non-recursive median filters.

Separable recursive median filter:

$$y_{i,j} = \text{med}(y_{i,j-v}, \dots, y_{i,j-1}, z_{i,j}, \dots, z_{i,j+v}),$$

$$z_{i,j} = \text{med}(z_{i-v,j}, \dots, z_{i-1,j}, x_{i,j}, \dots, x_{i+v,j}).$$



s the weighted L_1

Weighted median is the estimator T that minimizes the weighted L_1 norm:

$$\sum_{i=1}^{n} w_i |x_i - T| \to \min.$$

It is described by:

 $y_i = med\{w_{-v} \ {}^{\circ}x_{i-v}, \dots, w_v \ {}^{\circ}x_{i+v}\},\$

where $w \, x$ denotes duplication of x, w times to $\{x, ..., x\}$.

n

Multistage median filter:



$$y_{i,j} = med(med(z_1, z_2, x_{i,j}), med(z_3, z_4, x_{i,j}), x_{i,j}),$$

$$z_{1} = \operatorname{med}(x_{i,j-\nu}, \dots, x_{i,j}, \dots, x_{i,j+\nu}),$$

$$z_{2} = \operatorname{med}(x_{i-\nu,j}, \dots, x_{i,j}, \dots, x_{i+\nu,j}),$$

$$z_{3} = \operatorname{med}(x_{i+\nu,j-\nu}, \dots, x_{i,j}, \dots, x_{i-\nu,j+\nu}),$$

$$z_{4} = \operatorname{med}(x_{i-\nu,j-\nu}, \dots, x_{i,j}, \dots, x_{i+\nu,j+\nu}).$$

It preserves edges in horizontal, vertical and diagonal directions.

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Order Statistics Filters



Ranked order filters:

An *r*-th ranked filter y_i output is the *r*-th order statistic of signal x_i samples $\{x_{i-\nu}, \dots, x_i, \dots, x_{i+\nu}\}$, $n = 2\nu + 1$ that exist in a *running filter* window.

- It introduces a strong bias in the estimation of the mean, when the rank is small or large (tending to *min* or *max filters*).
- The bias is even stronger when the input data have a long-tailed distribution.



Order Statistics Filters



Max/min filters:

Running maximum $x_{(n)}$ and **minimum** $x_{(1)}$ are the two extremes of the ranked-order filters.

- Maximum filter effectively removes negative impulses in an image.
- Minimum filter removes positive impulses.
- Both filters fail in the removal of mixed impulse noise.
- Both filters have good edge preservation properties (but shift edges).
- Max/min filters tend to enhance bright and dark image regions, respectively.




Max/min filters



a) Baboon image corrupted by mixed impulsive noise;b) The output of a cascade of max and min filters [PIT2000].



Order Statistics Filters *Running implementation of max filter*.



$y_{i} = \begin{cases} x_{i}, & \text{if } x_{i} \ge y_{i-1}, \\ y_{i-1}, & \text{if } x_{i} < y_{i-1} \text{ and } x_{i-n} < y_{i-1}, \\ \max(x_{i}, \dots, x_{i-n+1}), & \text{if } x_{i} < y_{i-1} \text{ and } x_{i-n} = y_{i-1}. \end{cases}$

- In average, only 3 comparisons are needed.
- A similar algorithm exists for min filtering.



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α-trimmed mean filters:



It rejects α% of the smaller and α% of the larger observation data.
It is a compromise between the median filter and the moving average filter for varying α.

• Its performance is poor for short-tailed distributions.





Midpoint filter.

$$MP = \frac{1}{2} \left(x_{(1)} + x_{(n)} \right)$$

is optimal for uniform noise.





Modified trimmed mean filter (MTM):

$$y_{ij} = \frac{\sum \sum_{A} a_{rs} x_{i+r,j+s}}{\sum \sum_{A} a_{rs}},$$

$$a_{rs} = \begin{cases} 1, & |x_{i+r,j+s} - \text{med}\{x_{ij}\}| \le q \\ 0, & \text{otherwise.} \end{cases}$$

- MTM trims out pixels deviating strongly from the local median.
- It removes outliers.





Double window modified trimmed mean (DW MTM):

• A variation of MTM, it uses two different sized filter windows to achieve good robustness and edge preservation.

Modified nearest neighbour filter (MNN):

$$a_{rs} = \begin{cases} 1, & |x_{i+r,j+s} - x_{ij}| \le q \\ 0, & \text{otherwise.} \end{cases}$$

- MNN trims out pixels deviating strongly from the central pixel value.
- It has good edge preservation properties.



L-filter (or L-order statistic) definition:



Location Invariance constraint.

$$\sum_{j=1}^{n} a_j = \mathbf{a}^T \mathbf{e} = 1, \qquad \mathbf{e} = [1, ..., 1]^T.$$



In the case of additive noise:

$$x_i = s_i + n_i,$$

coefficient vector a can be obtained after the MSE minimization:

$$MSE = E\{(s_i - y_i)^2\} = E\left\{\left(\sum_{j=1}^n a_j x_{(j)} - s_i\right)^2\right\} = \mathbf{a} \ \mathbf{R}^T \mathbf{a},$$
$$\mathbf{a} = \frac{\mathbf{R}^{-1} \mathbf{e}}{\mathbf{e}^T \mathbf{R}^{-1} \mathbf{e}}.$$

• **R**: $n \times n$ correlation matrix of vector $\mathbf{n} = [n_{(1)}, ..., n_{(n)}]^T$.





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- The optimal L-filter:
 - for Gaussian noise is the moving average.
 - for Laplacian noise is the median filter.
 - for uniform noise is the midpoint.
- L-filter has no streaking effects, provided that its coefficients are not similar to those of the median filter.
- It has greater computational complexity than both the median and the moving average filter.





- Midpoint filters optimal estimators in the case of additive white uniform noise.
- Arithmetic moving average filters are optimal estimators in the case of additive white Gaussian noise *N*(0,1):

$$f_X(x) = \frac{1}{\sqrt{2\pi}} \exp\{-\frac{x^2}{2}\}.$$

 Median filters are optimal estimators in the case of additive white Laplacian noise:

$$f_X(x) = \frac{1}{2}e^{-|x|}$$



Digital Image Filtering

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Adaptive Order Statistic Filters Minimal Mean Square Error (MMSE) filter:



$$x_{ij} = s_{ij} + n_{ij}$$
.

- It is an *adaptive filter*:
 - It performs like arithmetic mean in homogeneous image regions.
 - It performs no filtering close to edges.

• It preserves edges, as it does not filter the noise in edge regions. • Various choices of the local measures of \hat{m}_{χ} , σ_{χ}^2 , σ_{n}^2 . • Various choices of the local measures of \hat{m}_{χ} , σ_{χ}^2 , σ_{n}^2 .

Adaptive Order Statistic Filters Decision-directed filters:



- They take into account both edge and noise information.
- Impulses, when detected, can be removed from the estimation of the local mean, median and standard deviation.
- When an edge is detected, the window of the filter can become smaller, so that edge blurring is minimized.
- Adaptive window edge detection (AWED) filter:
 AWED filter window size/shape can be adapted.



Adaptive Order Statistic Filters

Modified

Median Filter

Window Adaptation

Signal-adaptive median (SAM) filter:

• It is an adaptive filter based on the two-component image model:

$$y_{1ij} = \widehat{m}_x + b_{ij}(x_{ij} - \widehat{m}_x).$$

$$y_{ij} = r^{-1}(y_{1ij}).$$

 It has excellent performance in noise filtering, edge and image detail preservation.



 $r^{-1}()$

b_{ii}

Impulse Detection

Estimation





Two-component model filters



a) Original image;
 b) Image corrupted by Gaussian noise (variance=100) and mixed impulsive noise; c) SAM filter output [PIT2000].



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Image intensity f(i,j) can be considered as **pixel temperature** that can be diffused over the entire image domain, in an iterative process described by f(i,j,t) over various steps t.

Isotropic diffusion filtering can perform image smoothing:

$$\frac{\partial f}{\partial t} = c \operatorname{div}(\nabla f) = c \left(\frac{\partial^2 f}{\partial x^2} + \frac{\partial^2 f}{\partial y^2} \right)$$

- c: diffusion coefficient.
- Diffusion is also used for image segmentation.

Limitations:



- While it smooths noise, isotropic diffusion filtering also blurs important image features, such as edges.
- As iteration number increases, the image will tend to a constant mean average image, hence destroying all image information.
- It dislocates edges, when moving from finer to coarser scales (correspondence problem).
- Some smoothing properties of linear diffusion filtering are only suitable for 1D filtering.





Anisotropic diffusion depends on local image properties, e.g., local image edges.

• It reduces diffusion at image edges:

 $\frac{\partial f}{\partial t} = \operatorname{div}((c(f)\nabla f).$

- div: divergence operator.
- ∇f : image f(i, j, t) differentiation (edge detection) at iteration t.
- Diffusion close to edges is reduced, because of the form of c(f):

 $c(f) = \frac{1}{1 + \frac{|\nabla f|^2}{2}}, \qquad \lambda > 0.$





Anisotropic image diffusion equation:

$$\frac{df(i,j,t)}{dt} = div(c(i,j,t)\nabla f) = c(i,j,t)\Delta f + \nabla c\nabla f.$$

• Δ : Laplacian operator.

It performs simultaneous noise reduction and contrast enhancement across image regions, while deriving consistent deterministic scale-space image descriptions.

It smooths homogeneous image regions while retaining image edges.

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The 4-nearest North, South, East and West neighbors of the Laplacian operator can be used:

$$f(i,j,t+1) = f(i,j,t) + \lambda [c_N \nabla_N f + c_S \nabla_S f + c_E \nabla_E f + c_W \nabla_W f](i,j,t).$$

0 ≤ λ ≤ ¹/₄: ensures numerical stability.
∇_N, ∇_S, ∇_E, ∇_W are nearest-neighbor differences:

$$\begin{aligned} \nabla_N f(i,j,t) &\triangleq f(i-1,j,t) - f(i,j,t), \\ \nabla_S f(i,j,t) &\triangleq f(i+1,j,t) - f(i,j,t), \\ \nabla_E f(i,j,t) &\triangleq f(i,j+1,t) - f(i,j,t), \\ \nabla_W f(i,j,t) &\triangleq f(i,j+1,t) - f(i,j,t). \end{aligned}$$

- Iterating this scheme can be thought as moving towards coarser image resolutions in *scale-space*.
- Diffusion coefficients are updated at every iteration as a function of the image intensity gradient:

$$c_{N}(i,j,t) = g\left(\left\|\nabla f\left(i+\frac{1}{2},j,t\right)\right\|_{2}^{2}\right),\\c_{S}(i,j,t) = g\left(\left\|\nabla f\left(i-\frac{1}{2},j,t\right)\right\|_{2}^{2}\right),\\c_{E}(i,j,t) = g\left(\left\|\nabla f\left(i,j+\frac{1}{2},t\right)\right\|_{2}^{2}\right),\\c_{W}(i,j,t) = g\left(\left\|\nabla f\left(i,j-\frac{1}{2},t\right)\right\|_{2}^{2}\right).$$

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a) Original image; b-d) Various anisotropic diffusion iterations.







a) Original Byzantine painting with cracks.

- b) Localized cracks.
- c) Filled cracks using anisotropic diffusion.

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Image interpolation is an important operation with many applications:

- Image zooming (e.g., for video games)
- Image upsampling (e.g., in neural autoencoders or in neural semantic region segmentation.
- Image magnification/upsampling.
 - Video format conversion.





Zero-order (hold) interpolation: pixel (x, y) is assigned the value of the geometrically closest pixel in the image array:

$$f_i(n_1, n_2) = f([n_1/2], [n_2/2]).$$

- Repeated application: zooming by a factor of $2^n \times 2^n$.
 - For large *n*, regions of constant intensity (image blobs) are visible.
- It is sometimes used in video effect creation.



VML

Linear interpolation:

$$f(x,y) = (1 - \Delta_1) (1 - \Delta_1) f(n_1, n_2) + (1 - \Delta_1) \Delta_2 f(n_1, n_2 + 1) + \Delta_1 (1 - \Delta_2) f(n_1 + 1, n_2) + \Delta_1 \Delta_2 f(n_1 + 1, n_2 + 1),$$



- It is a first-order polynomial interpolation.
- It produces smoother interpolated images.

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where:



In *p*-order interpolation, the image is interpolated with zeros:

$$f'(n_1, n_2) = \begin{cases} f(\frac{n_1}{p}, \frac{n_2}{p}) & \text{if } n_1 = pk, n_2 = pl \\ 0 & \text{otherwise.} \end{cases}$$

Then, image f' is convolved p times with convolution matrix H.
Example of a convolution matrix H:

$$\mathbf{H} = \begin{bmatrix} 1/4 & 1/2 & 1/4 \\ 1/2 & 1 & 1/2 \\ 1/4 & 1/2 & 1/4 \end{bmatrix}$$

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BABOON Image.







Zero-order interpolation.

Linear Interpolation.





Cubic spline Interpolation.

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Neural image filtering

A classic autoencoder consists of:

- Encoder layers
- Latent View Representation (code)
- Decoder layers



Autoencoder architecture.





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Neural image filtering



Tries to:

- Encode the input from a corrupted version of it
- Undo the effect of the corruption process



Data corruption typically in 30-50% of the pixels

In the loss function the output values are compared with the original input & not the corrupted output!

Artificial Intelligence & Information Analysis Lab Denoising Autoencoder.



Neural image filtering



Medical image denoising using convolutional denoising autoencoders.

Objective:

Denoise medical images as a preprocessing step in medical image analysis

Methodology:

- Combination of convolutional, denoising & stacked autoencoder
- 2 datasets used, consisting of 722 high resolution images
- Gaussian & Poisson distribution introduced, with various noise proportion.




Neural image filtering

Medical image denoising using convolutional denoising autoencoders







Neural image filtering





Image de-raining [DER2023].





Neural image filtering





Image de-fogging.

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Thank you very much for your attention!

More material in http://icarus.csd.auth.gr/cvml-web-lecture-series/

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